



Harper Grace Hospitals
Harper Hospital Division

July 18, 1985

U.S. Nuclear Regulatory Commission
Region III
Materials Licensing Branch
799 Roosevelt Rd.
Glen Ellyn, IL. 60137

Re: Control No. 79162

Dear Mr. Mideria:

In reference to our phone conversation on Wednesday, July 17, 1985, concerning our amendment for establishment of a Regional Cerebral Blood Flow Laboratory, I have attached the following items that you requested: 1) Standard rCBF Clinical Protocol, 2) Literature concerning the Harshaw System 400.

As we discussed, the extreme sensitivity of this diagnostic procedure will not tolerate a leakage of Xenon-133 gas in excess of a few percent of the administered dose. It is for this reason that extra protective measures such as those listed as "Specific steps taken to minimize 133 Xenon leakage" within the enclosed clinical protocol are taken. Therefore, due to the sensitivity of this procedure and the extra protective measures taken, we request that our leakage rate of 10%, which is noted in parts 5 and 6 of our amendment application, be approved and our amendment granted.

If you have any further questions or require any additional information, please contact me.

Sincerely,

Thomas M. Kumpuris, M.S.
Thomas M. Kumpuris, M.S.
Nuclear Medical Physicist

TMK:do

cc: Roger Higgins, Ph.D.
Curtis Smith
J. Muz, M.D.

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21-04127-02 PDR

3990 John R., Detroit, Michigan 48201

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STANDARD rCBF CLINICAL PROTOCOL

Regional Cerebral Blood Flow Analysis (rCBF) is a noninvasive quantitative measurement of cerebral hemodynamics.

The method has been used for:

1. Management of critically injured patients (head trauma)
2. Evaluating patients for extracranial/intracranial bypass (superficial temporal to middle cerebral artery bypass)
3. Diagnosis of migraine
4. Evaluation of carotid endarterectomy
5. Evaluation of strokes

Normal subjects and category 4 and 5 patients (above) will be tested at Harper Hospital.

The normal procedure:

1. The purpose of the procedure, its investigational or diagnostic nature, the apparatus and the approximate length of the testing period are all explained.
2. The appropriate consent form is signed by the subject.
3. Hair clips, earrings or other head adornments are removed. A disposable paper cap is placed on the subjects head for hygienic purposes. The subject is placed supine on a stretcher.
4. A close-fitting, comfortable face mask is selected and located over the subjects mouth and nose. Careful

selection of the appropriate face mask is a key step in the elimination of gas leakage during the study. The face mask is held in place by careful adjustment of the elastic retainers.

5. The subject is allowed a ten minute acclimatization period before the test is started.
6. The subjects head is carefully positioned within the probe holder helmet (the probes are initially locked in a withdrawn position). The position of the helmet in relation to bony landmarks is carefully adjusted. Each probe is advanced until it presses lightly against the scalp without discomfort to the subject. Each probe is locked in place.
7. A corrugated plastic tube is used to connect the face mask to the gas delivery/extraction device. The subject is allowed to adjust to the new situation.
8. The delivery unit is charged with ^{133}Xe to a concentration of approximately 12 mci/litre (requires approximately 30 mci load).
9. The data collection program is initiated and the subject unknowingly inhales a ^{133}Xe and air mixture for one minute.
10. At the end of this period the subject is switched to breathing room air and the expired gases are collected in an activated charcoal filter within the

delivery/extraction unit. The build up of radio activity within the filter is measured and displayed on the collection device. Alarms are fitted to indicate impending filter saturation.

11. At the end of the washout period (15 minutes including 1 minute of inhalation) the test is concluded. The probes are withdrawn from the subjects head, the face mask is removed and the subject allowed to sit up.
12. A brachial blood pressure is taken and 3 millilitres of blood drawn for hemoglobin and PCO_2 determinations.

Specific steps take to minimize ^{133}Xe leakage:

1. Careful subject selection: only cooperative, conscious, coherent subjects will be tested.
2. The nature of the study will be carefully explained, particularly the need to remain still to ensure a leak free mask/face junction.
3. Difficult mask fitment may be overcome by the use of suitable gap-filling material (uncooked pancake batter). Subjects with beards and moustaches may be required to shave.
4. A suitable fan may be mounted above and behind the helmet in such a way that any ^{133}Xe gas would be blown away from the scintillation detector in order to minimize extraneous contamination and to provide the subject with a less claustrophobic environment during

the study.

5. A suitable ^{133}Xe leakage monitor, Xenogard, will be located in the testing area and will be in operation during the study.
6. ^{133}Xe will not be stored in the testing area.
7. Appropriate air supply and extraction rates will be maintained in order that, should a leak occur, the leak will be confined to the study room and not spread to adjacent areas.
8. Appropriate documentation of isotope use, background activity and cumulative exposure will be maintained.

SYSTEM 400™ INTRODUCES QUANTITATIVE AND FUNCTIONAL
ICBF MEASUREMENT PLUS ADVANCED XENON DELIVERY.



HARSHAW

About Hamshaw and rCBF

As the world's leading producer of nuclear radiation detection and related electronic components, Hamshaw has been a major contributor to the science of nuclear medicine.

As the discipline has matured, Hamshaw has continued as a prolific contributor of supportive equipment and expertise, including the first system specifically designed for nuclear medicine and clinical applications.

By the early 1970's, thousands of Hamshaw applications designed for detection were in the field, many of them being applied to laboratory and clinical investigations of regional cerebral blood flow — rCBF.

The logical evolution of Hamshaw's early work in rCBF analysis was the production of the world's first complete rCBF system, including software, hardware, and capability to compare and contrast results.

In 1975, this goal was achieved with the introduction of the first complete computer-based rCBF analysis system by the Baylor College of Medicine in Houston, Texas. Although this system was later replicated, it is still in daily operation, having performed over 7000 rCBF studies to date.



ICBF: QUANTITATIVE MEASUREMENT OF CEREBRAL HEMODYNAMICS

The Hamshaw rCBF System provides quantitative functional information unobtainable by alternate investigative procedures. In fact, an important rCBF application is demonstration of the effects of structural abnormalities identified by CT, ultrasound, angiography and scintillation camera studies.

Other methodologies for measuring cerebral hemodynamics have included positron emission tomography (PET), single photon emission computed tomography (SPECT), multiprobe analysis (MFA), and CT using non-radioactive Xenon. While these methodologies have some merit for rCBF analysis, Hamshaw MFA has demonstrated superior clinical practicality in terms of safety and simplicity of procedure.

A Vital Diagnostic Tool

In addition to demonstrating the hemodynamic effects of structural lesions, rCBF is a vital diagnostic tool for:

- management of critically injured patients
- Head Trauma
- evaluation of normal pressure hydrocephalus (NPH)
- evaluation of cerebral aneurysms
- CT hypoxia
- diagnosis of stroke or myocardial infarction
- diagnosis of cerebral vascular disease
- diagnosis of dementia

Non-Invasive Methodology

A drive mask is placed over the patient's nose and mouth. As the patient relaxes in a supine position,

his head is placed in the transparent probe holder. Probes are then inserted into the holder in a symmetrical configuration.

The patient breathes a Xenon-133 mixture for one minute, followed by a 10-14 minute washout period breathing room air. During this period, the head probes transfer the uptake and washout of Xenon-133.

The entire patient procedure — which is routinely performed by nuclear medicine or general medicine technicians — takes approximately 20 minutes.

The computer analyzes the data and generates gray flow, white flow and other diagnostic parameters.

Xenon-133 Safe and Convenient

Xenon-133 is an inert, non-toxic, non-radioactive gas. It is produced by the decay of Uranium 235. It is an isotope of Xenon, a noble gas, and is chemically inert. It is physiologically inert except for transient increases at high concentrations.

Extensive diagnostic use has been made of Xenon-133 in nuclear medicine for evaluation of pulmonary function and lung imaging. It is physiologically inactive in seconds, provides concentrations, no contraindications are known, and no adverse reactions specifically attributable to Xenon-133 have been reported.

Xenon-133 has a half-life of 5.31 days. It is supplied in a gas in break-sealed glass ampules and can be shipped anywhere in the world by container, either

INTRODUCING THE NEW HARSHAW rCBF SYSTEM 400.

With the introduction of the System 400, Harshaw again moves the leading edge of rCBF technology a significant step forward.

Designed to simplify operation while it expands application and analyzing capabilities, the key features of this unique system offer many for performance benefits.

- **Helmet Probe Holder** provides reproducible probe positioning for serial studies. ■ **New Xenon Delivery System** accommodates even patients on life support. ■ **Visual Software** displays data on a video screen. ■ **Control Console** simplifies operation. ■ **Optical Scan System** provides accurate collimation. ■ **Integration of IV Monitoring** provides maximum flexibility in study design. ■ **Scalable Data** expands to 3000 measurements. ■ **Compact** Harshaw requires less floor space.

Advanced new Xenon delivery unit. The Xenon-133 delivery unit incorporated in Harshaw's complete rCBF System was specifically designed to satisfy demands for more surgical than traditional pulmonary ventilation-perfusion units previously used. It incorporates an air-ventilator valve for controlled ventilation and an oxygenator for hyperventilation and support of the patient.

The System 400's ability to deliver a constant flow of xenon to the patient's head is a major safety feature. It is called the "shadow" feature because of its low dead volume, the hyperventilating sub-ject because of its efficient Xenon recycling system, and the patient's requirement for breathing assistance because it can be connected to any separator having an external exhalation valve with controller.

For the most efficient use of Xenon-133, patients receive the Xenon from a closed circuit. Since recirculating type systems can suffer O₂ depletion, provision is made for automatic oxygen re-perfusion. The system maintains a constant flow of the same O₂ concentration used in the patient's ventilation for rCBF studies at the life-support patient.

An activity concentration meter calibrated in microcuries (mc) ensures economical Xenon usage, an important consideration at high case loads.

Selectable inhalation or intravenous injection.

The two methodologies for non-invasive measurement of rCBF are Xenon-133 inhalation and IV injection, with inhalation being the most often used.

Both methods yield essentially the same final results, while IV injection may be selected for patients with impaired pulmonary function who might not tolerate a standard Xenon-133 inhalation.

Because the Harshaw System 400 is fully controlled, the user merely pushes a button to automatically adjust system operation for either inhalation method.

Head probes.

The design of the head probes used in the System 400 reflects Harshaw's 30 plus years' experience in nuclear

detector technology. Rugged, reliable, lightweight and well-shielded from background radiation and electromagnetic interference, these probes meet all rCBF performance requirements.

Harshaw's probes incorporate a 1/2" diameter by 3.4" thick NaI(Tl) detector and a photomultiplier in a stainless steel housing. A gold foil window allows the probe to be sterilized and exchanged. The collimator has a 5/8" mach to the probe's length, bore attachment by 1"

Three detector collimator diameters are selected for the optimum sensitivity/spatial resolution ratio.

Helmet probe holder and stand.

The combination of helmet probe holder and portable stand assures reproducible probe positioning, both height and angle of the helmet

assembly are adjustable to accommodate patient position.

The reproducible probe positioning is the most efficient means of acquiring rCBF data and permits rCBF measurements to be performed even on patients lying on a gurney. The lightweight assembly is readily moved out of room traffic when needed.

The transparent construction of the helmet permits precise positioning of the head probes perpendicular to the scalp. The helmet is easily moved to the patient and is

reproducible probe positioning is particularly advantageous for serial studies. When in place, the probes are securely held by retaining collars, secured with lock screws, which provide additional shielding for the head probes, reducing the effects of scattered radiation.



COMPUTERIZED OPERATION FOR FAST, ACCURATE ICBF MANAGEMENT.

Graphic display assists in data interpretation.

A 30 channel ICBF study yields more than 200 items of ICBF-related information. And making graphic display presentation a primary tool for data interpretation.

Some of the information presented on the ICBF display is based on a computerized analysis of opposing head probes and various other brain hemodynamic mean values (1)(2). Often greater variance from normal values since a great deal of information has been published in the literature about "normal" values (3)(4). To serve both schools of thought, Hazbrow software offers the user a choice of two graphic display formats.

The first format portrays a single hemodynamic profile with opposing head probes represented as a single square. The calculated value for each probe is placed within its respective half of the square. To simplify left-right comparison of measurements, all odd numbered probes are located on the patient's left hemisphere, and even numbered probes on the right.

The second display format incorporates an outline of each hemisphere with individual head probes represented as a square. To the right of each square is the calculated measurement for a particular study, and to the left is the "normal" value \pm one standard deviation. The "normal" values used

are the Baylor Normal (5), which are divided into decades of life to facilitate comparison. These "normals" are a composite of men and women without risk factors.

Hard copy unit.

The hard copy unit can be used to reproduce any information which is displayed on the computer terminal, but is normally used for permanent data summation charts and graphic displays. Since files may involve five or more pages of summation, Hazbrow's ICBF System uses a plain paper electronic copy unit to quickly and easily produce desired hard copies at a speed of ten seconds per page.

"Application designed"

The Hazbrow 430 electronics were designed for ICBF application. Even personnel with limited experience in nuclear medical electronics can operate this system. Digital gain, stabilization, which ensures accurate energy calibration, is an example of this design philosophy.

Interchangeable plug-in modules are used in each head probe channel, permitting the user to correct system malfunctions should they occur. This reduces downtime and service calls.

Energy centerline and window width settings for all channels are accomplished with common controls and controlled in key for ease of operation.

New software reduces analysis time.

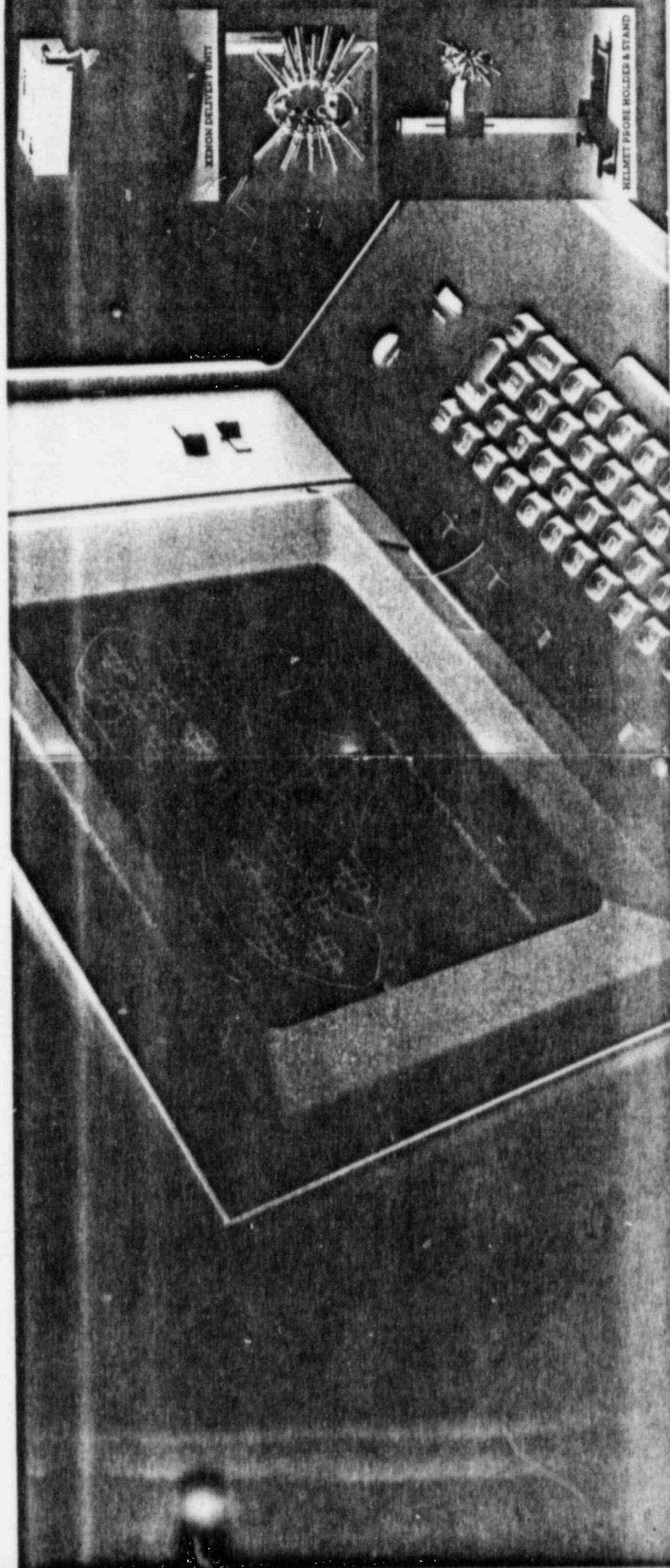
Hazbrow software utilizes the variable menu algorithm developed by Fletcher (6) and recommended by Cernat (7). It is written in Fortran IV and implemented under the DEC PDP-11* operating system. Analysis speed is an important consideration, both in high patient volume and serial study situations.

*Digital Equipment Corp., Maynard, MA.

"Menu-driven" controls simplify operation.

Hazbrow's ICBF software is written in menu-driven format for ease of operation. This plus software control of all functions - including the Xenon delivery unit - greatly reduces the time necessary to establish operator familiarity.

In the menu format, operator interaction with the System 430 is based on a series of simple questions displayed on the computer screen. The questions and responses are structured in a logical sequence requiring minimal operator education.



TOTAL COMPUTERIZED SYSTEM SUPPORT.

Digital gain stabilization.

This feature is unique to the System 400. With its many years of experience in nuclear radiation detection and RCB, Hamshaw recognized early that a fast and accurate method of calibration was necessary in an RCB system, consisting of many as 32 detectors.

Digital gain stabilization automatically adjusts individual detector amplifier gain, maintaining even if a detector gives more pulses than is attainable by other means. It ensures accurate calibration even by personnel whose experience with nuclear radiation detectors is limited.

Computer selection.

Since the Hamshaw RCB System is totally software controlled, the computer is a functional element, not limited to data analysis. In fact, part of the analysis is electronics and hardware. The computer can be selected to control the computer, or the computer can be selected to control the electronics.

This means consideration of sub-system components or off-line analysis is impractical. Selection of the appropriate computer involves consideration of the entire computational package, including the terminal, data storage

medium, interfacing to data acquisition electronics, hard copy device and software.

The entire package must be selected to operate together and perform the task with acceptable accuracy and reliability. When the computer has a 16-32 or 64K byte memory, it is essential if the package meets your objectives.

The DEC LS-11* microprocessor has shown itself a practical choice in terms of speed, cost and operational flexibility when used in the System 400.

*Digital Equipment Corp., Maynard, MA

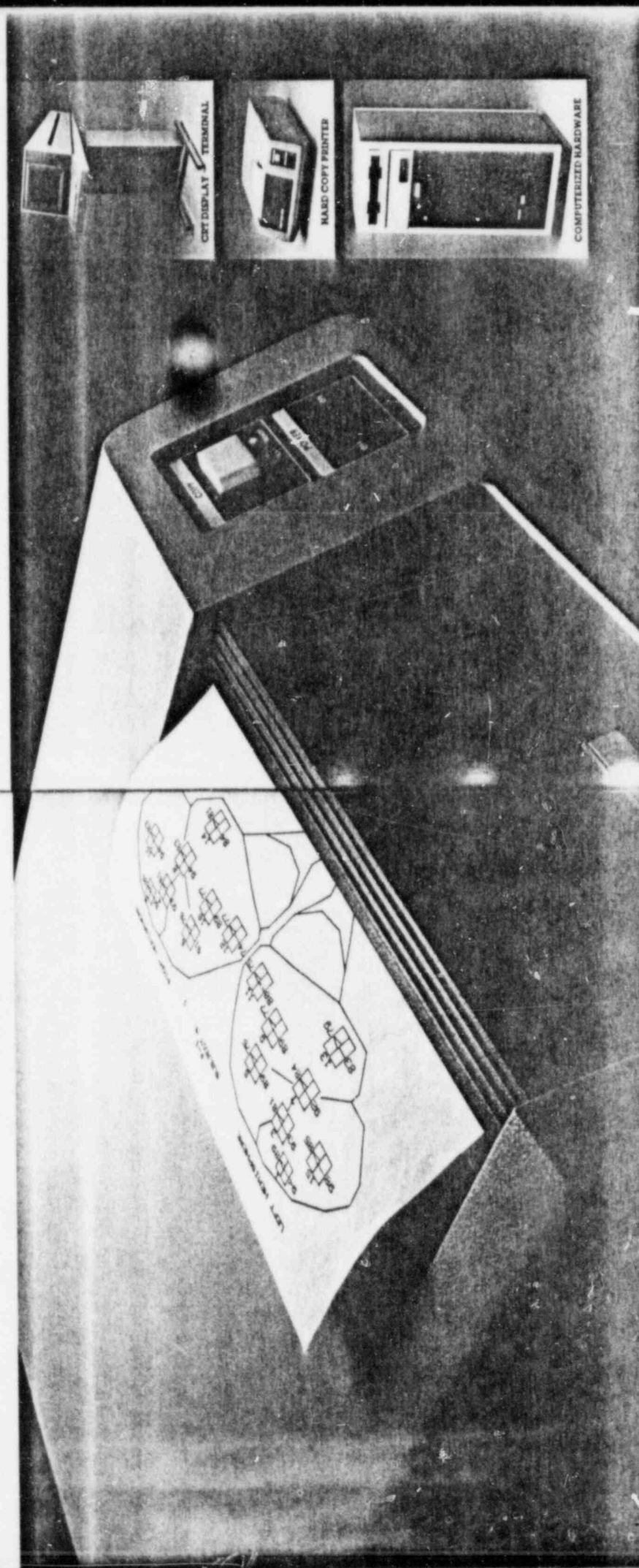
Compact hardware requires less floor space.

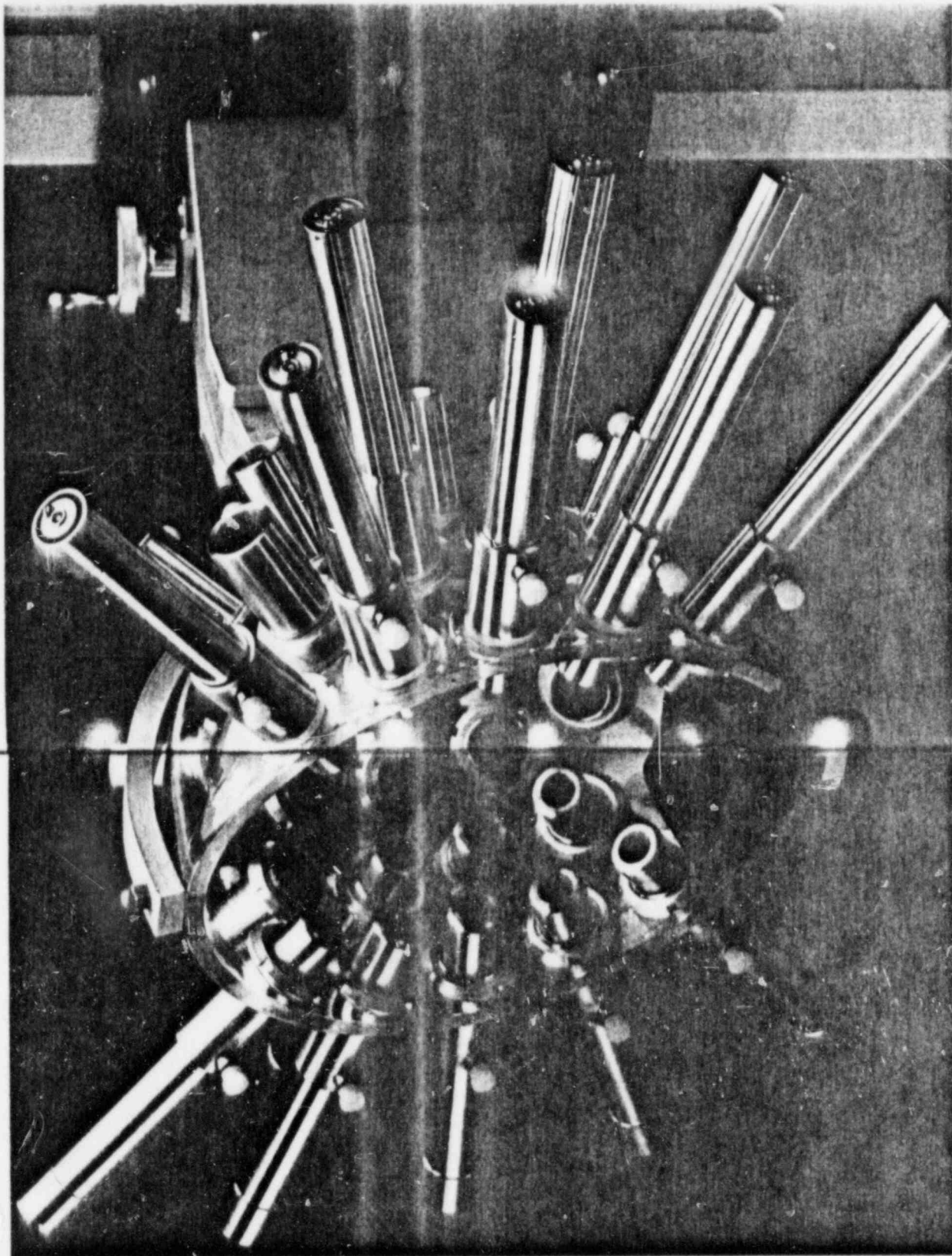
The modularity of the Hamshaw System 400 computer permits you to expand the system as little as 64 square feet (6 square meters) of floor space. Because of its mobility, installation in intensive care is common.

Hamshaw provides complete system support. System 400 brings all the computer functions needed to add various RCB analysis together in a system designed for top performance and backed by superior service. Technical assistance and replacement parts are available world-wide within as little as 24 hours.

Complete on-site installation and customer training are provided by Hamshaw technicians. Clinical applications and other technical data are periodically provided with our change.

For complete details on how Hamshaw can bring your clinical and research RCB analysis capabilities to the next level of performance, call or write to arrange an appointment in your laboratory or clinic.





Footnotes:

1. Paulson, O. B. Regional Cerebral Blood Flow in Allopexy Due to Occlusion of the Middle Cerebral Artery. *NEUROLOGY* 20:63-77, 1970.
2. Fierst, E., Des Rosiers, M. Cerebral Blood Flow Measurements at Stroke. In: *Brain Research* (ed. CERESEAL). APTICAL DISEASE, London, Churchill Livingstone, 1976, pp. 85-106.
3. McHenry, L. C., Jr., Metry, J. et al. Xenon-133 Inhalation Method for Regional Cerebral Blood Flow Measurements: Normal Values and Test Series Results. *STROKE* 9:346-360, 1978.
4. Nunnally, H., Meyer, J. S., et al. Effects of Advancing Age on Regional Cerebral Blood Flow. *ARCHIVES OF NEUROLOGY* 36:410-416, 1979.
5. These values are derived from participants in the longitudinal study of aging in cerebral vascular disease under the auspices of J. S. Meyer, M.D., and T. Shaw, Ph.D., Veterans Administration Medical Center, Division of Cerebral Vascular Research, Houston, Texas.
6. Fletcher, P. A New Apparatus for Simultaneous Multiple Measurements. *COMPUTER* 11:317-322, 1970.
7. Grant, W. D., Thompson, H. K., Jr., Meyer, J. S., et al. Regional Cerebral Blood Flow Estimated by Xenon-133 Inhalation. *STROKE* 9:245-250, 1978.

These data are believed to be accurate but are not guaranteed to be so. Nothing herein shall be construed as suggesting the use of our product in violation of any laws, regulations or rights of third parties. Buyer should evaluate accuracy and safety of product before use. We do not warrant that our product will be used in connection with our product unless a contract is entered into with our company.

CONVERSATION RECORD

TIME

DATE

6/19/85

T/PE

☐ VISIT

☐ CONFERENCE

☒ TELEPHONE

☐ INCOMING

☒ OUTGOING

Location of Visit/Conference:

NAME OF PERSON(S) CONTACTED OR IN CONTACT WITH YOU

ORGANIZATION (Office, dept., bureau, etc.)

TELEPHONE NO.

Tom Kompuris, HP

Harper-Grace Hosp.

313/494-9381

SUBJECT

Xenon-133 amendment

494-8417

ROUTING

NAME/SYMBOL

INT

SUMMARY

① Your calculations for concentrations of Xe-133 in restricted areas and unrestricted areas use an assumed loss rate of 10% which is too low. Calculations should use a 20% loss rate.

② The concentrations in restricted areas using 20% seem to produce adequate results, but the results of calculations using 20% loss rate in unrestricted areas are slightly higher than NRC requirements.

a.) Submit new calculations:

1. use 20% loss and

2. you should either:

a.) increase exhaust or

b.) lower per patient dose (20mCi) or

c.) decrease number of studies

~~d.) increase room volume~~

Note: Xenon is vented to the outside via stack

ACTION REQUIRED

License must respond in 30 days w/ weighting unit control # 79162

NAME OF PERSON DOCUMENTING CONVERSATION

SIGNATURE

DATE

JR Made

6/19/85

ACTION TAKEN

SIGNATURE

TITLE

DATE